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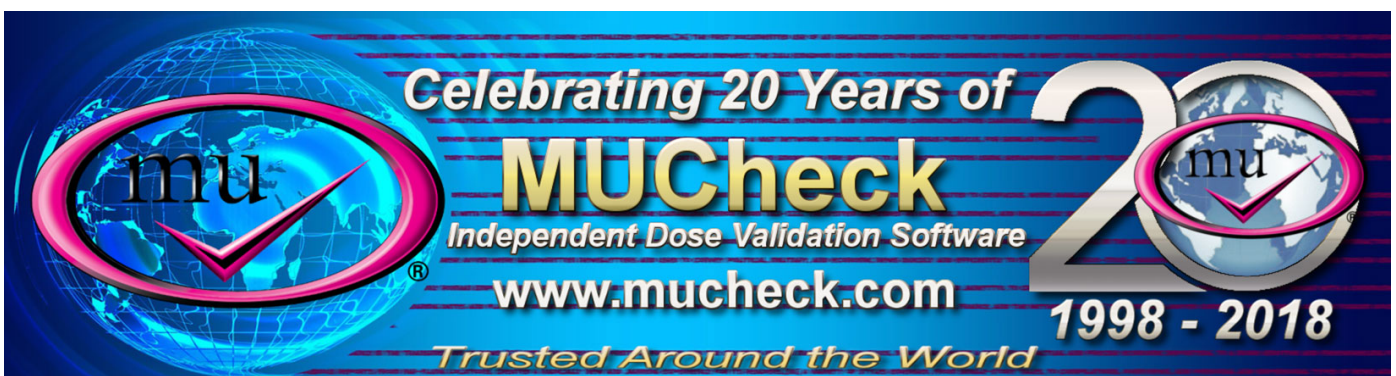
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# Water-dispersible magnetite nanoparticles as $T_2$ MR imaging contrast agent

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## Abstract

Water-dispersible iron oxide nanoparticles (NPs) consistently demonstrated a significant interest in the field of biomedical applications. Through this report, we present the synthesis of monodispersed magnetite NPs with an excellent water-dispersibility by employing a modified thermal decomposition method. Synthesized NPs were characterized by x-ray diffraction, transmission electron microscopy, x-ray photoelectron spectroscopy, vibrating sample magnetometry and cytotoxicity assay. From the results, it is evident that the NPs are highly crystalline, of spherical morphology with diameters of  $20 \pm 1$  nm, superparamagnetic, and cytocompatible. Finally, we probed NPs as a  $T_2$ -weighted contrast agent in magnetic resonance Imaging which resulted in relatively high  $r_2$  values. Therefore, the NPs could be effectively used as a potential candidate for various biological applications.

## 1. Introduction

In the past two decades, magnetic nanoparticles (NPs) showed considerable importance in the medical applications [1] because of its interesting physico-chemical properties [2]. Among these NPs, magnetite NPs (MNPs) are widely employed for various biological applications such as drug delivery, hyperthermia, and magnetic resonance imaging (MRI) [3, 4]. However, to effectively use MNPs in said applications, the important criteria are that the NPs must be water-dispersible [5], monodispersed with narrow particle size, high crystallinity, biocompatible, and so forth [2]. Thus, the researchers tend to use reactants that are expensive and toxic, such as surfactants and solvents [6]. Therefore, it is always remained as a great challenge to design a simple method for synthesizing highly water-dispersible MNPs.

There are very few reports available on the synthesis of water-dispersible MNPs by thermal decomposition (TD) method. In general, this technique involves using multiple reactants such as triethylene glycol [5], diethylene glycol [7], 1,2-hexadecanediol

[8], 1,2-dodecanediol [9], oleic acid, octyl ether, oleylamine, phenyl ether, hexadecane, eicosene, and dioctyl ether [10]. Furthermore, the above protocol requires a ligand-exchange process to make the NPs as hydrophilic, essentially using surfactants such as polyethylene glycol [11], pluronic F127, [12] silica [13], and cetyltrimethylammonium bromide (CTAB) [14–22].

In our case, we have combined the above procedures into a one-pot technique to directly synthesize water-dispersible MNPs without the necessity of ligand-exchange process. The synthesis involves using benzyl ether as a solvent assisting in reducing the metal precursor, and CTAB, the widely used cationic surfactant, to provide a surface charge to prevent the NPs from being agglomerated. However, the major disadvantage of CTAB is its toxicity. Nevertheless, this could be completely minimized by using it appropriately [23]. In this report, we have discussed the synthesis and characterization of water-dispersible  $\text{CTA}^+$  stabilized magnetite nanoparticles (C-MNPs) and investigated the cell viability by MTT [3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium

bromide] assay [24], as well as the possibilities of using them as a potential  $T_2$  contrast agent.

## 2. Materials and methods

### 2.1. Materials

All the chemical reagents were purchased from Sigma-Aldrich, Mexico and used without further purification, unless or otherwise stated; iron (III) acetylacetonate ( $\text{Fe}(\text{acac})_3$ ,  $\text{Fe}(\text{C}_5\text{H}_7\text{O}_2)_3$ ,  $\geq 99.9\%$ ), hexadecyltrimethylammonium bromide (CTAB,  $\text{CH}_3(\text{CH}_2)_{15}\text{N}(\text{Br})(\text{CH}_3)_3$ ,  $\geq 99\%$ ), benzyl ether (BE,  $(\text{C}_6\text{H}_5\text{CH}_2)_2\text{O}$ ,  $\geq 98\%$ ), dimethyl sulfoxide (DMSO,  $(\text{CH}_3)_2\text{SO}$ ,  $\geq 99.9\%$ ), ethanol (EtOH,  $\text{CH}_3\text{CH}_2\text{OH}$ ,  $\geq 99.8\%$ ), and MTT ( $\text{C}_{18}\text{H}_{17}\text{N}_5\text{S}$ ,  $\geq 97\%$ ). Cell culture reagents like Dulbecco's Modified Eagle Medium (DMEM), fetal bovine serum, and streptomycin were purchased from Gibco, Thermo Fisher Scientific Inc.

### 2.2. Synthesis of CTAB stabilized magnetite nanoparticles (C-MNPs)

C-MNPs were synthesized by employing modified protocol of TD technique. Initially, 2 mmol of  $\text{Fe}(\text{acac})_3$  was dissolved in 20 ml of BE in a three-neck round-bottom flask; to this is added CTAB with various molar concentrations (0.1, 0.2, and 0.3 M). The reaction was carried out with the aid of heating mantle to provide uniform heating throughout the flask. The refluxing was carried out at  $260^\circ\text{C}$ , under continuous and vigorous stirring in a nitrogen atmosphere ( $\text{N}_2$  atm) for one hour, and was naturally cool down to room temperature. Subsequently, 150 ml of EtOH was added to precipitate the C-MNPs. Later, the solution was centrifuged (at 4000 rpm, for 15 min) to remove excess CTAB. The black pellet-like residue was collected and washed with EtOH. The resultant material was dispersed in de-ionized water and was stored until further use.

### 2.3. Characterization techniques

The structure and crystallinity of the C-MNPs were probed by PAN analytical, X'Pert Powder x-ray diffractometer (XRD) using  $\text{Cu-K}\alpha$  radiation ( $\lambda = 0.154$  nm) with  $2\theta$  angles ranging from  $10^\circ$  to  $90^\circ$  at a scan rate of 0.02/1 s. The sample was prepared by drop-casting few drops of C-MNP solution onto the glass substrate. The morphology and size of C-MNPs were analyzed using both Low (TEM, Jeol JEM-2100) and high-resolution transmission electron microscopy (Jeol ARM200F). The TEM sample grid was prepared by placing a drop of water-dispersed C-MNPs onto the carbon film 300 mesh copper grid (Ted Pella, Inc.), and was dried in a vacuum desiccator over anhydrous calcium sulfate for 24 h prior to the analysis. The NP hydrodynamic size was measured using dynamic light scattering (DLS) technique by employing Zetasizer Nano ZS90 (Malvern Instruments) on C-MNPs samples in deionized water at a

wavelength of 633 nm at  $25^\circ\text{C}$ . Thermogravimetric analysis was carried out using a TGA Q50 (TA Instruments) from  $30^\circ\text{C}$  to  $600^\circ\text{C}$  at a heating rate of  $10^\circ\text{C min}^{-1}$  in a  $\text{N}_2$  atm to study the % weight loss of NPs. Further to evaluate the magnetization and magnetic behavior, magnetic hysteresis loops were recorded for a known amount of NPs in the sample holder under the applied field of  $-7500$  to  $7500$  Oe by using Vibrating Sample Magnetometry (VSM, Quantum Design, PPMS DynaCool). X-ray photoelectron spectroscopy (XPS) analysis was conducted to identify the elemental composition and their oxidation states using a K-Alpha XPS System (Surface Analysis, Thermo Scientific) equipped with monochromated  $\text{Al-K}\alpha$  x-ray source. The XPS data were calibrated using the binding energy of C1s.

### 2.4. MRI analysis

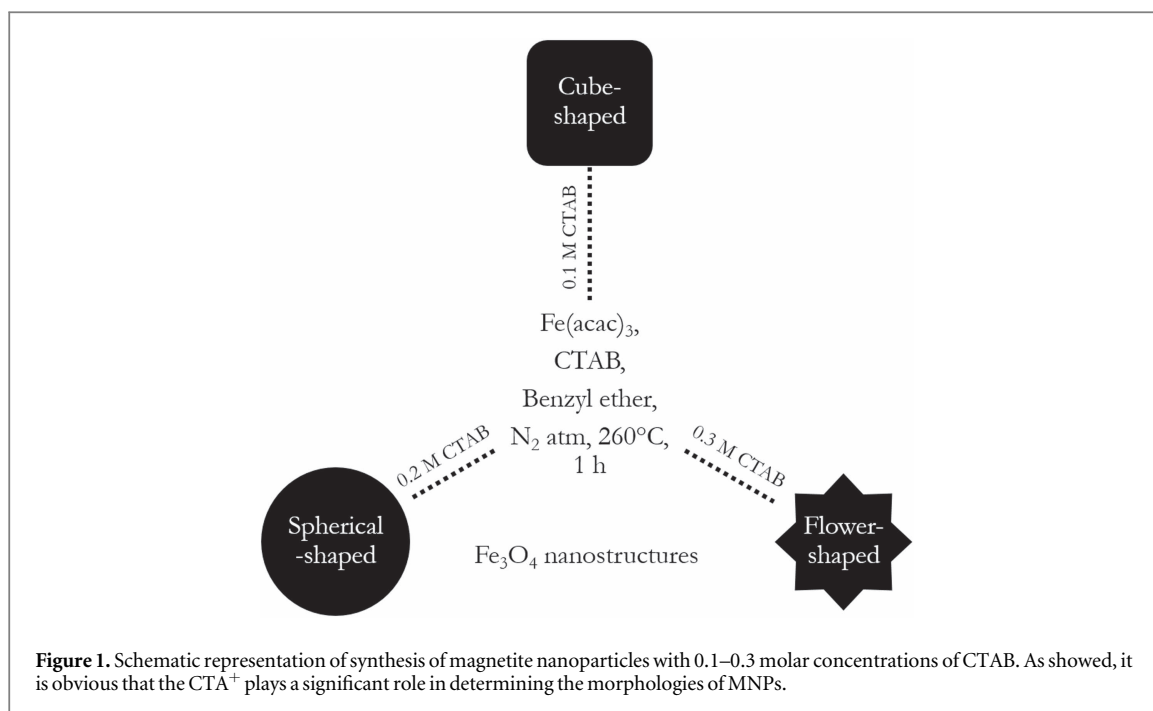
MRI experiments were performed on a 7 T scanner (Clinical Signa HDxt scanner Varian). Known concentrations of C-MNPs were dispersed in 2 ml of water in an Eppendorf tube.  $T_2$ -weighted images were obtained using the following parameters; repetition time (TR) = 2000 ms, echo time (TE) = 15 ms, with a resolution of  $256 \times 256$  points, and a slice thickness of 4 mm at room temperature. For  $T_1$  measurements, spin-echo sequences with a constant TE of 24 ms and varying TR from 50 ms to 5 s were used.

### 2.5. Cell viability assay

Cell viability studies were performed using MTT assay as given below:

- Both L6 (skeletal muscle cell line) and Hep2 cells (laryngeal carcinoma cell line) were cultured in DMEM supplemented with 10% fetal bovine serum and  $100 \mu\text{g ml}^{-1}$  streptomycin in an incubator with 5%  $\text{CO}_2$  atmosphere at  $37^\circ\text{C}$ .
- Cells were seeded into a 12-well plate at a cell density of  $1 \times 10^5$  cells/plate.
- Subsequently, various concentrations ( $50 - 250 \mu\text{g ml}^{-1}$ ) of C-MNPs were added.
- Then, a  $10 \mu\text{l}$  of MTT ( $5 \text{ mg ml}^{-1}$ ) in DMEM was added and incubated for 3 h.
- After incubation, excess MTT solution was removed, and a  $200 \mu\text{l}$  of DMSO was added to dissolve the formazan crystals.
- The plates were kept on a shaker for 10 min followed by 24 h incubation.
- Later, absorbance was recorded at 570 nm using an iMark microplate reader (Bio-Rad Laboratories).

The measurements were recorded in triplicates and viability data was obtained from their average values.



### 3. Results and discussions

The main aim of this synthesis was to produce highly monodispersed, readily water-dispersable, and importantly biocompatible MNPs using CTAB. It is well-known that CTAB is employed to synthesize various metal NPs with precise morphologies [25–27] resulting in smaller and uniform NPs [28] by specific interaction with lattice planes [29]. The growth of an NP is determined by two factors that affect the crystal facets [30, 31], viz.,

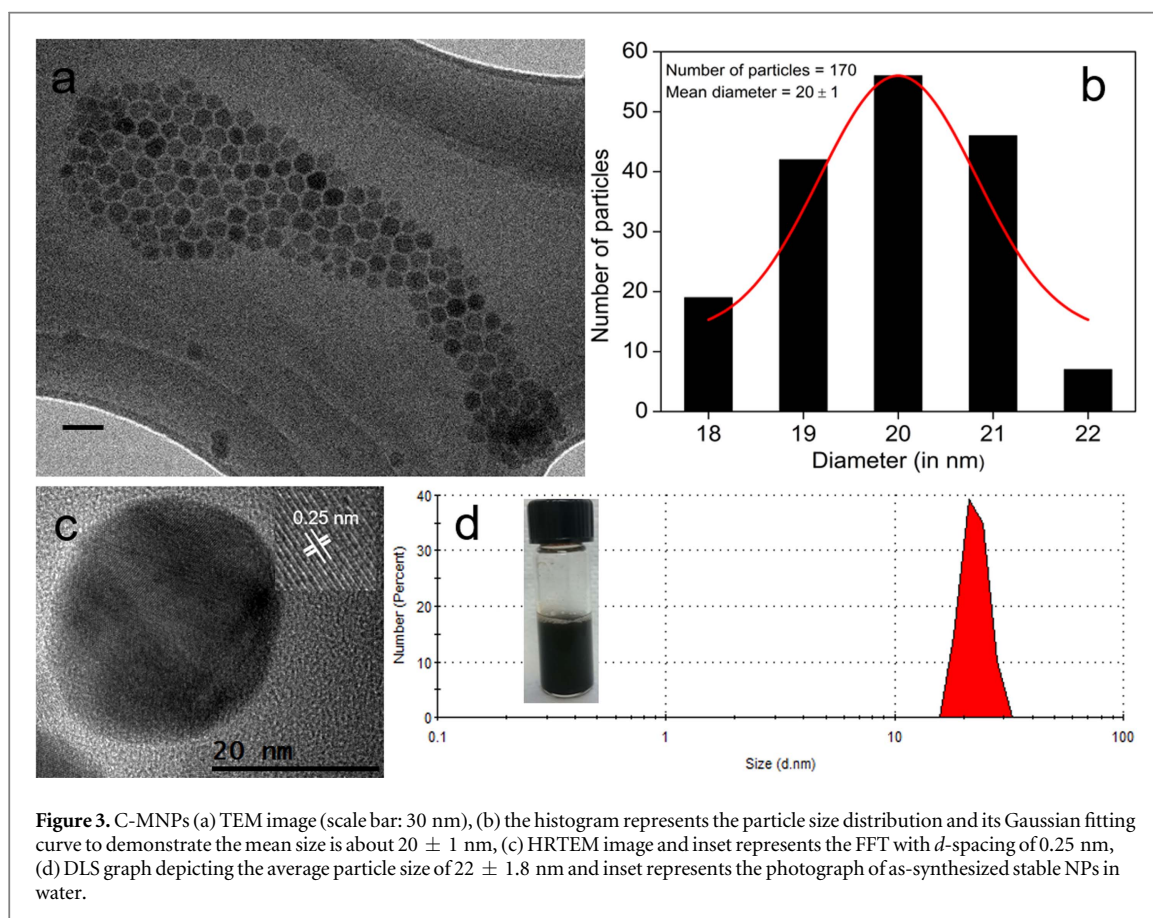
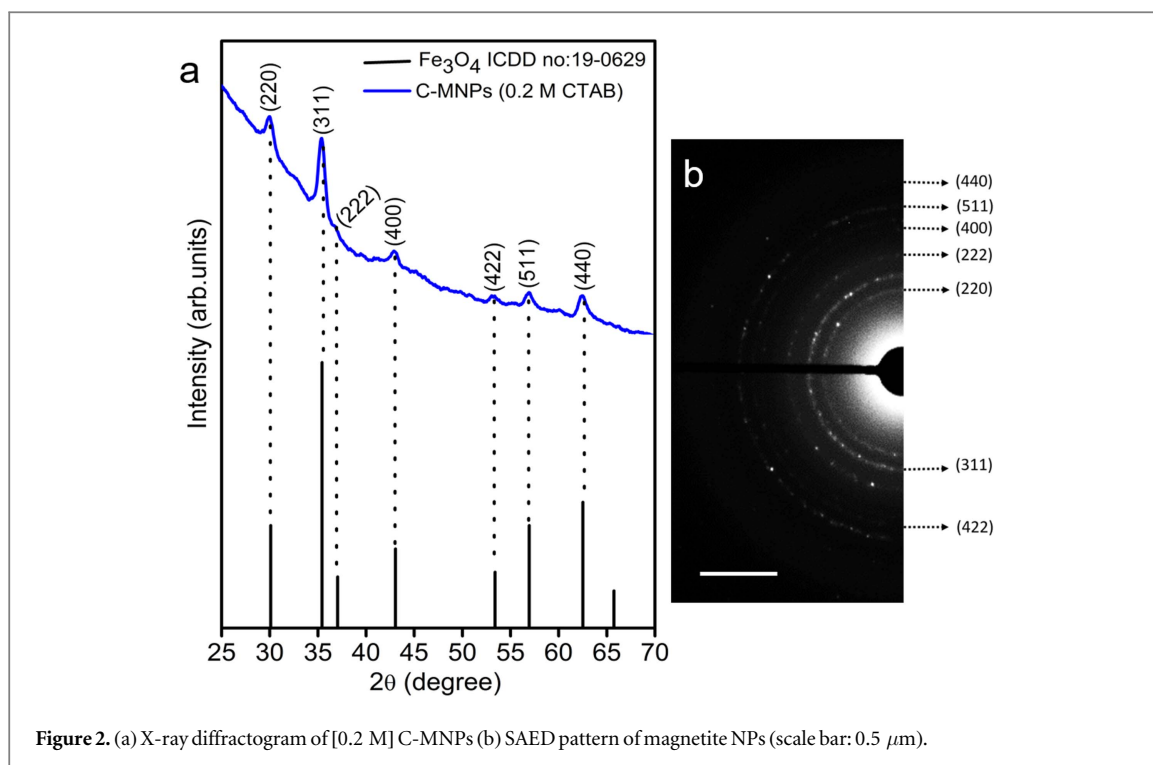
- Thermodynamically controlled: uniform growth (spherical structures), e.g., spherical NPs
- Kinetically controlled: preferential/directional growth (anisotropic structures), e.g., rods, cubes, prisms.

Usually, the morphology of an NP is affected during the process of crystallization by the selective binding of surfactant moieties in the various positions of the crystal [32–34]. Therefore, considering the function of the surfactant; the as-synthesized NPs (spherical-morphology) was probed by several characterization techniques to study in-depth properties and to evaluate their possibility as a  $T_2$  contrast agent. Figure 1 depicts the facile method that we adapted for the synthesis of C-MNPs.

XRD pattern, as shown in figure 2(a), reveals the crystallinity of C-MNPs synthesized with 0.2 M CTAB. All peaks are well indexed to face-centered cubic  $\text{Fe}_3\text{O}_4$  lattice and are in corroboration with the International Centre for Diffraction Data reference pattern, no:19-0629. It is apparent from the pattern that there is no sign of secondary phase formation

which is clearly due to the maintenance of  $\text{N}_2$  atm throughout the reaction. The noisy and amorphous background in the pattern corresponds to the amorphous glass substrate [35]. The average crystallite size has been calculated using Scherrer formula [36], considering the spherical shape of the NPs, as 16.4 nm, and is in corroboration with TEM analysis. The diffraction rings from the selected area electron diffraction pattern corresponds to the MNPs, as represented in the inset of figure 2(b), which also confirms the crystallinity of the NPs [5].

Figure 3(a) shows the transmission electron (TE) micrographs revealing the formation of spherical morphologies of C-MNPs synthesized with 0.2 molar concentrations of CTAB. The distorted cubical, and flower-like morphologies of C-MNPs synthesized with 0.1, and 0.3 molar CTAB concentrations, respectively are shown in figures S1(a) and (b) in the ESI. It is apparent that the addition of CTAB has clearly affected the NPs formation by producing a series of morphologies with precise growth in the ‘nm’ range. Sayed *et al* reported the formation of similar nanostructures when CTAB was employed in the synthesis of magnetite NPs [37]. The possible formation mechanism of the various morphologies is as explained below: in case of cube, the morphology is minorly distorted and the edges were indistinct. It is due to the insufficient reaction time [38], even though the  $\text{CTA}^+$  ions initiated the directional growth by anchoring to  $\text{Fe}_3\text{O}_4$  surface [39]. Therefore, the synthesis time have to be prolonged to obtain monodisperse cube shaped NPs. The spherical shape formation is mostly energy based during the NPs growth process. Due to high concentration of surfactant moieties onto the surface of metal seeds, it leads to less surface energy on NPs. Therefore, as the surface energy of spherical NPs is very low when



compared to other anisotropic NPs, the possibility is comparatively higher to form spherical shaped NPs [40]. The flower-shaped NPs is due to the self-assembly/clustering of individual NPs which assemble from the centre to form a multicore flower structure [41].

Therefore, from the above interpretation, it is evident that CTAB plays a dual role as both coating and shape-directing agent [42].

In this report, we have concentrated only on the synthesis and characterization of spherical NPs as it is

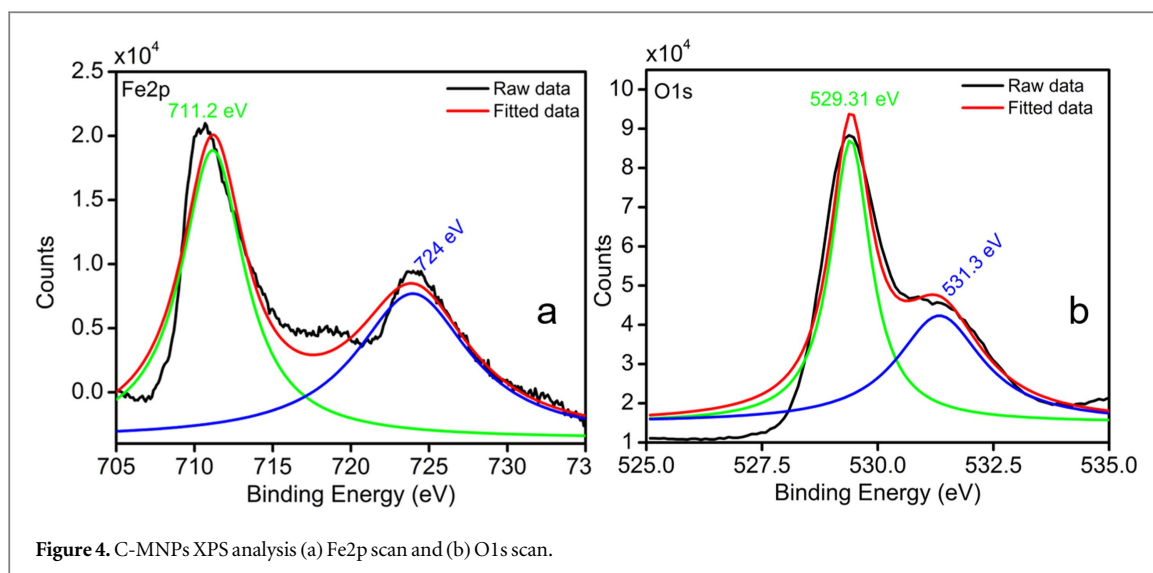


Figure 4. C-MNPs XPS analysis (a) Fe2p scan and (b) O1s scan.

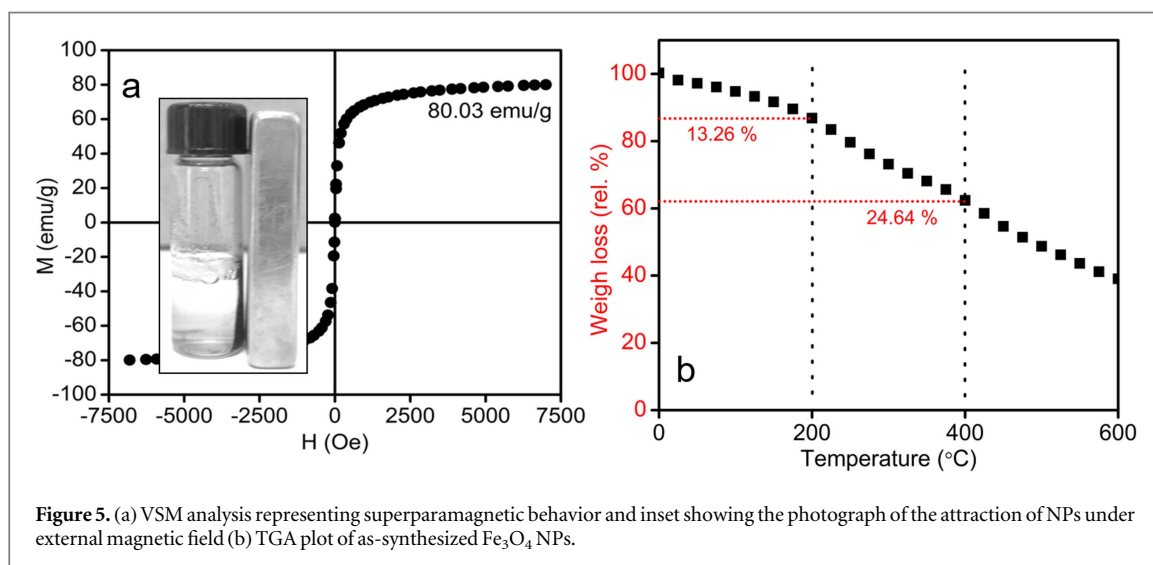


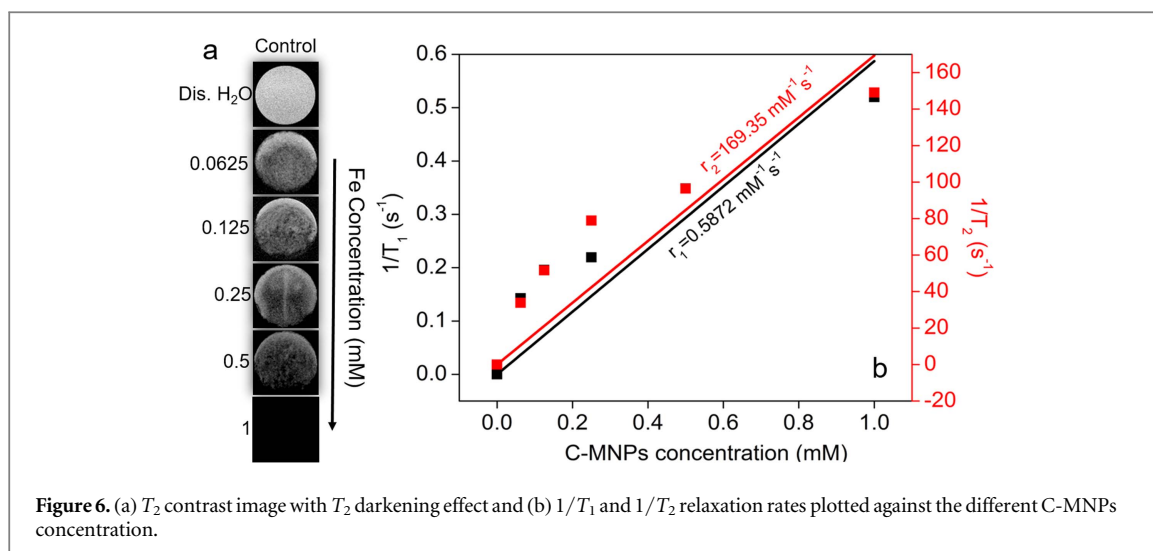
Figure 5. (a) VSM analysis representing superparamagnetic behavior and inset showing the photograph of the attraction of NPs under external magnetic field (b) TGA plot of as-synthesized  $\text{Fe}_3\text{O}_4$  NPs.

widely employed for biological applications [43], whereas further investigations are needed for distorted cubical and flower-like nanomaterials. TEM micrograph in figure 3(a) shows the spherical morphology of the C-MNPs exhibiting monodispersity, and non-aggregation. The reason behind the non-aggregation is due to the electrostatic repulsion among the head groups of  $\text{CTA}^+$  on the neighboring NPs. We manually measured the size of 170 NPs, using Gatan software (Digital Micrograph 3.7.0), and the distribution is as depicted in the histogram (figure 3(b)). The average size is thus calculated to be  $20 \pm 1$  nm. Figure 3(c) shows the HRTE micrograph of C-MNPs revealing it to be a single crystal [9], and corresponding inset depicts the fast Fourier transformation (FFT) image. The interplanar distance is measured, from FFT, to be 0.25 nm which corresponds to the (311) plane of the magnetite structure.

DLS analysis was performed on shelf stored water-dispersed C-MNPs to determine the particle's hydrodynamic size which plays a crucial factor for *in vivo* applications [44, 45]. The average hydrodynamic size

of NPs is found to be  $22 \pm 1.8$  nm (figure 3(d)), and the apparent increase in the relative size to TEM measurements is due to the adsorbing layer of  $\text{CTA}^+$  onto the NPs surface [5]. Inset in the figure 3(f) shows the photograph of the vial containing the colloidal C-MNPs in water.

The  $\text{CTA}^+$ 's adsorption on the NPs surface were investigated using XPS. The data (figures 4(a) and (b)) represents the core level spectra of Fe2p and O1s scans. Usually, MNPs exhibit two strong peaks at binding energies of 709 and 722.9 eV for Fe 2p<sub>3/2</sub> and Fe 2p<sub>1/2</sub> respectively [46]. However, in our case, Fe2p scan shows two strong peaks at 711.2 and 724 eV corresponding to Fe2p<sub>3/2</sub> and Fe2p<sub>1/2</sub> respectively with a minor shift in the binding energy values indicating the efficient adsorption of  $\text{CTA}^+$  onto the NP's surface. Moreover, the experimental data shows no peak at 719.0 eV, which additionally supports that the synthesized product is pure magnetite rather than maghemite. Furthermore, the O1s scan exhibited two strong peaks (529.31 and 531.3 eV) corresponding to the Fe-O bonding in magnetite [5, 47].



Magnetic measurements (figure 5(a)) revealed the superparamagnetic behavior of the NPs at room temperature with the magnetization value ( $M_s$ ) of  $80.03 \text{ emu g}^{-1}$  and a little remanence ( $M_r$ ) of ca.  $2.69 \text{ emu g}^{-1}$ . Magnetic NPs lesser than 20 nm exhibits superparamagnetic behavior with negligible remanence [48] which can strongly enhance the proton relaxation resulting to high  $r_2$  values [49, 50]. The remanence to saturation ratio ( $R = M_r/M_s$ ) was found to be 0.033. Nonetheless, the remanence ratio ( $M_r/M_s$ ) is lower than that expected for a ferromagnet ( $M_r/M_s = 0.8$ ) suggesting the source of anisotropy which is intrinsic magnetocrystalline anisotropy. However, this  $M_s$  value is comparatively higher than that of other MNPs, synthesized via TD method [7, 10] which could be attributed to the crystallinity of C-MNPs [51] due to its substantial impact on the  $M_s$  [52].

TGA measurements (figure 5(b)) depict that the NPs are stable even at higher temperatures. The initial weight loss of 13.26% up to  $200^\circ\text{C}$  signifies the evaporation of water molecules from the surface of NPs. The second weight loss (24.64%) from  $200^\circ\text{C}$  to  $400^\circ\text{C}$  may be attributed to the complete decomposition of organic CTAB moieties [53]. However, the weight loss from  $400^\circ\text{C}$  continues further which indicates the transformation of MNPs, to maghemite and may finally lead to hematite [54].

We effectively employed C-MNPs as a contrast agent in MR imaging using the 7 T scanner to investigate its property further. MR imaging is one of the finest tools used for non-invasive clinical diagnosis, due to its significant advantages such as high penetration depth and soft tissue contrast, to obtain images safely without any side-effects [55]. This technique distinguishes and improves the image quality of unhealthy lesions using contrast agents [56]. Figure 6(a) shows the  $T_2$  signal from the water-dispersed C-MNPs of different concentrations. It is observed that the signal intensity increases with the NPs concentration as seen

from the darkening effect. Therefore, this contrast enhancement is due to the exceptional properties of C-MNPs, such as size, shape, magnetic behavior, and so forth [57]. We have measured both transverse and longitudinal relaxivities. From which it is corroborated that these NPs express  $T_2$  imaging effect ( $r_2$  value =  $169.35 \text{ mM}^{-1} \text{ s}^{-1}$ ) rather than  $T_1$  ( $r_1$  value =  $0.5872 \text{ mM}^{-1} \text{ s}^{-1}$ ) by calculating the  $r_2/r_1$  ratio which is found to be 288.4. Figure 6(b) represents the relaxation rates  $1/T_1$  and  $1/T_2$  as a function of the NPs concentration. The  $r_2$  value is higher than the commercially available products. Such as, Ferumoxides (Feridex)  $r_2$  value of  $132 \text{ mM}^{-1} \text{ s}^{-1}$  at 7 T [58]. Moreover, also the  $r_2$  values (7 T) was 10-fold higher than that of CTAB stabilized MNPs which was  $15.4 \text{ mM}^{-1} \text{ s}^{-1}$  [20].

From the above studies, it is very clear that the synthesized C-MNPs satisfies to be a high-performance MR imaging probe [59] by fulfilling the following characteristics, such as,

- High saturation magnetization because of its high crystallinity,
- monodispersed NPs which can extend the circulation time in the blood pool,
- highly water-dispersible and biocompatible,
- particle size is less than 200 nm so it can easily be cleared by human spleen [60],
- proven to be relatively a better  $T_2$  contrast agent with high  $r_2/r_1$  ratio [12].

To evaluate the C-MNPs cytotoxic effects, we employed MTT assay to detect cell viability using normal L6 and cancerous Hep2 cells (figure 7). It is clearly observed that the presence of NPs in the medium does not affect the cells even at higher concentrations of  $250 \mu\text{g ml}^{-1}$ . Therefore, we can conclude that the NPs are highly cytocompatible by CTAB coating rather

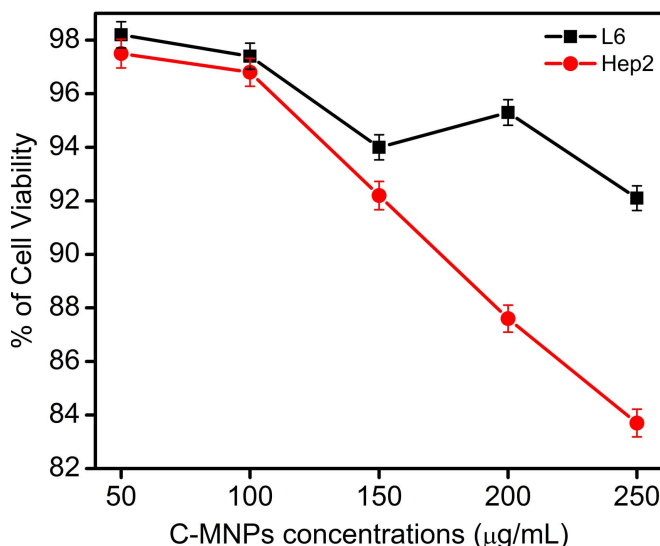


Figure 7. Cytotoxicity study of C-MNPs concentration using MTT assay with L6 and Hep2 cells.

than the naked NPs which usually release toxic ions and affects the biocompatibility [61]. Nevertheless, it is observed that the Hep2 cells exhibited a threshold limit of 80%, which as per our knowledge is due to the inherent capability of the NPs to stimulate apoptosis. Similar behavior was observed with MNPs in HepG2 and A549 cell lines [62].

#### 4. Conclusions

We have demonstrated a simple, and one-pot synthesis method for MNPs using CTAB. Importantly, these NPs are monodispersed and superparamagnetic as observed from TEM analysis and VSM measurements respectively. It is, therefore, evident that the surfactant CTAB has an essential role not only in defining the size of NPs but also acts as a shape determining factor. Additionally, these NPs are water-dispersible that can be readily usable for various biomedical applications without further surface modifications. MTT assay confirms the NPs are cytocompatible. Finally, we have evaluated their huge contrast enhancement in  $T_2$  weighted MR imaging. Therefore, we firmly believe that these MNPs can be used as a potential candidate for contrast imaging agents.

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